

Designation: F 1538 - 03

Standard Specification for Glass and Glass Ceramic Biomaterials for Implantation¹

This standard is issued under the fixed designation F 1538; the number immediately following the designation indicates the year of original adoption or, in the case of revision, the year of last revision. A number in parentheses indicates the year of last reapproval. A superscript epsilon (ϵ) indicates an editorial change since the last revision or reapproval.

1. Scope

- 1.1 This specification covers the material requirements and characterization techniques for glass and glass-ceramic biomaterials intended for use as bulk porous or powdered surgical implants, or as coatings on surgical devices, but not including drug delivery systems.
- 1.2 The biological response to glass and glass-ceramic biomaterials in bone and soft tissue has been demonstrated in clinical use $(1-12)^2$ and laboratory studies (13-17).
- 1.3 This specification excludes synthetic hydroxylapatite, hydroxylapatite coatings, aluminum oxide ceramics, alpha- and beta-tricalcium phosphate, and whitlockite.

2. Referenced Documents

- 2.1 ASTM Standards:
- C 158 Test Methods for Strength of Glass by Flexure (Determination of Modulus of Rupture)³
- C 169 Test Method for Chemical Analysis of Soda-Lime and Borosilicate Glass³
- C 373 Test Method for Water Absorption, Bulk Density, Apparent Porosity, and Apparent Specific Gravity of Fired Whiteware Products³
- C 623 Test Method for Young's Modulus, Shear Modulus, and Poisson's Ratio for Glass and Glass-Ceramics by Resonance³
- C 633 Test Method for Adhesion or Cohesive Strength of Thermal Sprayed Coatings⁴
- C 693 Test Method for Density of Glass by Buoyancy³
- C 729 Test Method for Density of Glass by the Sink-Float Comparator³
- C 730 Test Method for Knoop Indentation Hardness of Glass³
- C 958 Test Method for Particle Size Distribution of Alumina or Quartz by X-Ray Monitoring of Gravity Sedimentation³

- C 1069 Test Method for Specific Surface Area of Alumina or Quartz by Nitrogen Adsorption³
- C 1070 Test Method for Determining Particle Size Distribution of Alumina or Quartz by Laser Light Scattering³
- E 228 Test Method for Linear Thermal Expansion of Solid Materials with a Vitreous Silica Dilatometer⁵
- F 748 Practice for Selecting Generic Biological Test Methods for Materials and Devices⁶
- F 981 Practice for Assessment of Compatibility of Biomaterials for Surgical Implants with Respect to Effect of Materials on Muscle and Bone⁶

2.2 Code of Federal Regulations:⁷

Title 21, Part 820

2.3 United States Pharmacopoeia:⁸

Lead <252>

Mercury <261>

Arsenic <211>

Heavy Metals <231> Method I

2.4 U.S. Geological Survey Method:⁹

Cadmium

3. Terminology

- 3.1 Definitions of Terms Specific to This Standard:
- 3.1.1 *bioactive glass*—an amorphous silicate-based solid that is not intrinsically adhesive and that is capable of forming a cohesive bond with both hard and soft tissue when implanted, and will develop a hydroxycarbonate apatite layer when exposed to appropriate *in vitro* environments, such as simulated body fluid or tris-hydroxymethylaminomethane buffer.
- 3.1.2 *bioactive glass-ceramic*—an amorphous-derived crystalline silicate-based solid that is not intrinsically adhesive and that is capable of forming a cohesive bond with bone and soft tissue when implanted, and will develop a hydroxycarbonate

¹ This specification is under the jurisdiction of ASTM Committee F04 on Medical and Surgical Materials and Devices and is the direct responsibility of Subcommittee F04.13 on Ceramic Materials.

Current edition approved Apr. 10, 2003. Published May 2003. Originally approved in 1994. Last previous edition approved in 1994 as F 1538 – 94.

² The boldface numbers in parentheses refer to the list of references at the end of this specification.

³ Annual Book of ASTM Standards, Vol 15.02.

⁴ Annual Book of ASTM Standards, Vol 02.05.

⁵ Annual Book of ASTM Standards, Vol 14.02.

⁶ Annual Book of ASTM Standards, Vol 13.01.

⁷ Available from U.S. Government Printing Office, Superintendent of Documents, 732 N. Capitol St., NW, Mail Stop: SDE, Washington, DC 20401.

⁸ Available from United Stated Pharmacopia, 12601 Twinbrook Parkway, Rockville, MD 20852.

⁹ Crock, J.G., Felichte, F.E., Briggs, P.H., "Determination of Elements in National Bureau of Standards Geological Reference Materials SRM 278 Obsidian and SRM 688 Basalt by Inductively Coupled Plasma-Atomic Emission Spectrometry," *Geostandards Newsletter*, Vol 7, 1983, pp. 335-340.

apatite layer when exposed to appropriate *in vitro* environments, such as simulated body fluid or trishydroxymethylaminomethane buffer.

- 3.1.3 *bulk material*—intended to describe a unit material used as a load bearing implant.
- 3.1.4 *coating*—intended to describe a surface layer that is relatively thin compared to the overall dimensions of the prosthetic part that has been coated.
- 3.1.5 *glass biomaterial*—any one of a number of compositions of amorphous inorganic solids that are used as implant materials for various medical or dental uses, or both.
- 3.1.6 *glass-ceramic biomaterials*—any one of a number of compositions of an amorphous-derived crystalline solid that is used as an implantable biomaterial for medical or dental use, or both.
- 3.1.7 *particulate material*—intended to describe several pieces (usually small size) used together within an implant construct.

4. Chemical Requirements

- 4.1 Bulk compositions shall be tested using Test Method C 169.
- 4.2 The concentration of trace element levels in the bioactive glass and glass-ceramics shall be limited as follows:

Element	ppm, ma	
Arsenic (As)	3	
Cadmium (Cd)	5	
Mercury (Hg)	5	
Lead (Pb)	30	
total heavy metals (as lead)	50	

Either inductively-coupled plasma/mass spectroscopy (ICP/MS) (18), atomic absorption (AAS), or the methods listed in 2.3 and 2.4 shall be used.

5. Physical Characterization

- 5.1 The following physical and mechanical characterizations may be applicable to various bioactive glass and glass-ceramics products and should be used whenever possible to verify the material.
- 5.1.1 *Density*—The densities of glass and glass ceramic materials are related directly to the processing history and composition of the material. The density of the bulk material shall be measured using Test Methods C 373 or C 729 and shall be consistent for the specific materials.
- Note 1—This test should use a non-aqueous liquid for bioactive glass and glass ceramic materials, which are known to react in an aqueous environment and could thereby affect the measurement.
- 5.1.2 *Flexural Strength*—When used as bulk materials in load bearing applications, the flexural strength of the bulk material shall be measured using Test Methods C 158.
- 5.1.3 *Young's Modulus*—When used as a bulk material, Young's Modulus of glass and glass ceramic biomaterials shall be determined following Test Method C 623.
- 5.1.4 *Hardness*—Where applicable, for characterization of the material, the hardness of bulk samples shall be determined using Test Method C 730. The Knoop indentation hardness is one of many properties that is used to characterize glasses.

Attempts have been made to relate Knoop hardness to tensile strength, but no generally accepted methods are available. Such conversion is limited in scope and should be used with caution, except for special cases in which a reliable basis for conversion has been obtained by conversion tests.

- 5.1.5 Surface Area—The surface area of a particulate may be important in determining the reliability of the bioactivity of the material. Whenever the specific surface area of the material relates to function, the surface area of particulate glass and glass ceramic biomaterials shall be measured using Test Method C 1069.
- 5.1.6 Bond Strength of Glass or Glass Ceramic Coating—When used as a coating on a metallic or ceramic substrate, the bond strength of the coating shall be measured following Test Method C 633.
- 5.1.7 Crystallinity—For glass-ceramic biomaterials, the percent crystallinity and crystal phases present in glass ceramic biomaterials shall be determined by means of X-ray diffraction analysis. While there is no single standard method for determining the crystallinity and crystal phases of glass ceramic materials, techniques such as those detailed in Refs (19) and (20) should be followed to standardize methods as much as possible.
- 5.1.8 *Thermal Expansion*—Thermal expansion shall be measured using Test Method E 228, when materials are to be used for coatings (raw materials are to be measured), or on finished product as a quality control test.
- 5.1.9 *Particle Size*—When used as a particulate, the particle size shall be measured in accordance with Test Methods C 958 or C 1070.

6. Biocompatibility

6.1 Glass and glass-ceramic biomaterials should be evaluated thoroughly for biocompatibility before human use. Bioactive glass and glass-ceramic materials are unique in their mode of action when implanted in the body due to the released ionic species and the mechanisms by which these materials bond with bony tissue. These materials have been found to exhibit an excellent tissue response in laboratory studies (13-17) and clinical usage (1-12). Before any new formulations are used clinically, the tissue response should be characterized by the methods recommended in Practice F 748 and F 981 as appropriate.

7. Test Specimen Fabrication

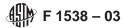
7.1 Test specimens should be prepared concurrent with implant devices, as well as from the same batch of material and by the same processes as those used in fabricating the glass and glass-ceramic implant device.

8. Quality Program Requirement

8.1 The manufacturer shall conform to Quality Systems requirements (2.2) or equivalent.

9. Keywords

9.1 bioactive glass; bioactive glass-ceramics; glass biomaterials; glass-ceramic biomaterial; surgical implants



APPENDIXES

(Nonmandatory Information)

X1. RATIONALE

X1.1 A number of glass-ceramic materials are available commercially. Bioactive glass and glass-ceramic materials are available commercially as synthetic graft materials for maintenance of the alveolar ridge; as devices for spinal fusion; as implants for replacement of the vertebral body, iliac crest, and ossicular chain of the middle ear; as bone filler to substitute for bone defects remaining after the excision of bone tumors and extraction of loosened joint prostheses; and as coatings on dental and orthopedic implants. As with any implant material, the bioresponse is critically dependent on the material properties. To achieve reliable biocompatibility, these properties must be known and consistent. This specification provides specifications for biocompatible grades of bioactive glass and glass-ceramics.

X1.2 In order to be called bioactive, the materials must demonstrate that living tissue is bonding to a significantly higher level than non-bonding implant control, as well as

demonstrate that ionic species are released from the material into solution in a controlled and reproducible manner.

X1.3 Bioactive glass and glass-ceramic materials are generally silicate-based materials, with additions of oxides of calcium, phosphorous, and various alkalis. They may be phosphate-based materials as well. These materials may also include fluoride and other alkaline earth metals. Table X1.1 gives a few specific examples of the bioactive glass and glass-ceramic materials produced. Since the compositions of these materials may vary greatly from product to product, it is not possible to specify their exact compositions.

X1.4 It is recognized that separate performance standards may be necessary for each end-use product. Physical and mechanical properties were not specified for this reason. A source of general test methods for glass and ceramic materials may be found in the *Annual Book of ASTM Standards*, Vol 15.02.

TABLE X1.1 Typical Bioactive Glass and Glass-Ceramic Compositions (Compositions in Weight %)

	**			
	45S5 Bioglass®	52S4.6 Bioglass®	S53P4 Bioactive Glass	A-W-GC (21)
SiO ₂	45	52	53.0	34.2
P ₂ O ₅	6	6	4.0	16.3
SiO_2 P_2O_5 CaO	24.5	21	20.0	44.9
CaF ₂				0.5
MgO				4.6
Na ₂ O	24.5	21	23.0	

X2. BIOCOMPATIBILITY

X2.1 No known surgical implant material has ever been shown to be completely free of adverse reactions in the human body. However, long-term clinical experience with the compositions referred to in this specification has shown that an acceptable level of biological response can be expected if the materials are used in appropriate applications.

REFERENCES

- Reck, R., "Tissue Reactions to Glass Ceramics in the Middle Ear," Clin. Otolaryngol, Vol 6, 1981, pp. 59–63.
- (2) Merwin, G. E., "Review of Bioactive Materials for Otological and Maxillofacial Applications," *Handbook of Bioactive Ceramics*, Vol 1, Ed. T. Yamamuro, L. L. Hench, and J. Wilson, CRC Press, Boca Raton, Florida, 1990, pp. 323–328.
- (3) Douek, E., "Otological Applications of Bioglass® Implants," Proceedings Fourth International Symposium on Bioceramics in Medicine, Ed. W. Bonfield, London, United Kingdom, September 10 and 11, 1990.
- (4) Stanley, H. R., et al., "Residual Alveolar Ridge Maintenance with a New Endosseous Implant Material," J. Pros. Dent., Vol 58, No. 5, November 1987.
- (5) Nakamura, T., et al., "A New Glass-Ceramic for Bone Replacement: Evaluation of its Bonding to Bond Tissue," *Journal of Biomedical Material Research*, Vol 19, 1985.
- (6) Yamamuro, T., et al., "Novel Methods for Clinical Application of Bioactive Ceramics," *Bioceramics: Material Characteristics Versus in Vivo Behavior*, Ann. New York Acad. Sci., Vol 523, 1988, pp. 107–114.
- (7) Yamamuro, T., "Reconstruction of the Iliac Crest with Bioactive Glass-Ceramic Prosthesis," *Handbook of Bioactive Ceramics Prosthesis*, Eds. T. Yamamuro, L. L. Hench, and J. Wilson, Vol 1, CRC Press, Boca Raton, FL, 1990, pp. 335–342.
- (8) Yamamuro, T., "Replacement of the Spine with Bioactive Glass-Ceramic Prosthesis," pp. 343–352, idem.
- (9) Taguchi, T., "A Bioactive Glass Powder-Ammonium Hydrogen Phosphate Composite for Repairing Bone Defects," *Journal of Appl. Biomater.*, Vol 1, pp. 217–223.
- (10) Froum, S.J., et al., "Comparison of Bioglass® Synthetic Bone Graft Particles and Open Debridement on the Treatment of Human Periodontal Disease," J. Periodontal., Vol 69, 1998, pp. 698-709.
- (11) Lovelace, T.B., et al, "Clinical Evaluations of Bioactive Glass in the Treatment of Periodontal Osseous Defects," *J. Periodontal.*, Vol 69, 1998, pp. 1027-1035.

- (12) Stoor, P., et al., "Bioactive Glass S53P4 in Repair of Septal Performations and Its Interactions with the Respiratory Infection-Associated Microorganisms Heamophilus influenzae and Streptococcus pneumoniae," J. Biomed. Mater. Res, (Appl. Biomater.), Vol 58, 2001, pp. 113-120.
- (13) Hench, L. L., and Paschall, H. A., "Histo-Chemical Responses at a Biomaterials Interface," *Journal of Biomedical Material Research*, Vol 5, 1974, p. 1.
- (14) Kitsugi, T., et al., "Bonding Behavior of a Glass-Ceramic Containing Apatite and Wollastonite in Segmental Replacement of the Rat Tibia Under Load-Bearing Conditions," *Journal of Bone St. Surg.*, Vol 71A, 1989.
- (15) Gross, U., et al., "The Response of Bone to Surface Active Glasses/Glass-Ceramics," CRC Critical Reviews in Biocompatibility, Vol 4, No. 2, 1988, pp. 155–179.
- (16) Piotrowski, G., et al., "Mechanical Studies of the Bone Bioglass® Interfacial Bond," *Journal of Biomedical Material Research*, Vol 6, 1975, p. 47.
- (17) Strunz, V., et al., "The Mechanical Strength of the Bond Between Bone and Implants of Glass-Ceramics with Apatite," *Dental Implants*, Ed. G. Heimke, Henser, Munich, 1980, pp. 27–34.
- (18) Northington, D.J., "Inductively Coupled Plasma-Mass Spectroscopy for the Analysis of Metals on Membrane Filters," *Am. Ind. Hyg. Assoc. J.*, Vol 48, 1987, pp. 977-979.
- (19) Cullity, B. D., *Elements of X-ray Diffraction*, 2nd ed., Addison-Wesley Publishing Company, Reading, MA, 1978.
- (20) Li, P., et al., "The Effect of Residual Glassy Phase in a Bioactive Glass-Ceramic on the Formation of its Surface Apatite Layer In-Vitro," *Journal Mater. Sci. in Med.*, Vol 3, 1992, pp. 452–456.
- (21) Kokubo, T., et al., "Apatite- and Wollastonite-Containing Glass-Ceramics for Prosthetic Application," *Bull. Inst. Chem. Res.*, Kyoto Univ., Vol 60, No. 3-4, 1982.

ASTM International takes no position respecting the validity of any patent rights asserted in connection with any item mentioned in this standard. Users of this standard are expressly advised that determination of the validity of any such patent rights, and the risk of infringement of such rights, are entirely their own responsibility.

This standard is subject to revision at any time by the responsible technical committee and must be reviewed every five years and if not revised, either reapproved or withdrawn. Your comments are invited either for revision of this standard or for additional standards and should be addressed to ASTM International Headquarters. Your comments will receive careful consideration at a meeting of the responsible technical committee, which you may attend. If you feel that your comments have not received a fair hearing you should make your views known to the ASTM Committee on Standards, at the address shown below.

This standard is copyrighted by ASTM International, 100 Barr Harbor Drive, PO Box C700, West Conshohocken, PA 19428-2959, United States. Individual reprints (single or multiple copies) of this standard may be obtained by contacting ASTM at the above address or at 610-832-9585 (phone), 610-832-9555 (fax), or service@astm.org (e-mail); or through the ASTM website (www.astm.org).